

The Wnt Inhibitor Sclerostin Is Up-regulated by Mechanical Unloading in Osteocytes *in Vitro**

Received for publication, December 11, 2014, and in revised form, May 5, 2015. Published, JBC Papers in Press, May 7, 2015, DOI 10.1074/jbc.M114.628313

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Background: Recent studies have suggested osteocytes as key players in mechanosensation and skeletal metabolism.

Results: Simulated microgravity induces an autonomous up-regulation of *SOST*/sclerostin and *RANKL*/*OPG* in a novel osteocytic cell line, Ocy454.

Conclusion: Mechanical loading regulates intrinsic osteocyte responses in concert with hormonal and cytokine inputs.

Significance: Learning how osteocytes sense mechanical loads would enable novel interventions to prevent disuse-induced bone loss.

Although bone responds to its mechanical environment, the cellular and molecular mechanisms underlying the response of the skeleton to mechanical unloading are not completely understood. Osteocytes are the most abundant but least understood cells in bones and are thought to be responsible for sensing stresses and strains in bone. Sclerostin, a product of the *SOST* gene, is produced postnatally primarily by osteocytes and is a negative regulator of bone formation. Recent studies show that *SOST* is mechanically regulated at both the mRNA and protein levels. During prolonged bed rest and immobilization, circulating sclerostin increases both in humans and in animal models, and its increase is associated with a decrease in parathyroid hormone. To investigate whether *SOST*/sclerostin up-regulation in mechanical unloading is a cell-autonomous response or a hormonal response to decreased parathyroid hormone levels, we subjected osteocytes to an *in vitro* unloading environment achieved by the NASA rotating wall vessel system. To perform these studies, we generated a novel osteocytic cell line (Ocy454) that produces high levels of *SOST*/sclerostin at early time points and in the absence of differentiation factors. Importantly, these osteocytes recapitulated the *in vivo* response to mechanical unloading with increased expression of *SOST* (3.4 ± 1.9 -fold, $p < 0.001$), sclerostin (4.7 ± 0.1 -fold, $p < 0.001$), and the recep-

tor activator of nuclear factor κ B ligand (*RANKL*)/osteoprotegerin (*OPG*) (2.5 ± 0.7 -fold, $p < 0.001$) ratio. These data demonstrate for the first time a cell-autonomous increase in *SOST*/sclerostin and *RANKL*/*OPG* ratio in the setting of unloading. Thus, targeted osteocyte therapies could hold promise as novel osteoporosis and disuse-induced bone loss treatments by directly modulating the mechanosensing cells in bone.

It has been recognized for over a century that mechanical loading is fundamental for the normal development and maintenance of the musculoskeletal system. Reduced loading is prevalent in our aging population, in the setting of spinal cord and other injuries, in prolonged bed rest, as a result of significant weight loss, or as experienced by astronauts during space flight and is invariably associated with bone loss (1–7). Although it has been appreciated for more than a century that bone models itself in response to its mechanical environment (Wolff's law) (8), the mechanisms underlying this response still need to be fully elucidated. Osteocytes are the most abundant but least understood bone cell type. Because osteocytes exhibit a dendritic morphology with extensive connectivity throughout the mineralized matrix of bone, it is thought that this system forms the bone mechanosensor, acting as the orchestrator of osteoblast and osteoclast activity in response to mechanical stimuli (9–11). Osteocyte ablation results in a resistance to disuse-induced bone loss, highlighting the central role osteocytes play as the mechanosensor of bone (12). Improved understanding of the molecular mechanisms of osteocyte mechanosensation could have significant implications for the treatment of bone disorders including osteoporosis, fracture healing, and disuse-induced bone loss.

The precise mechanisms whereby osteocytes respond to and convert mechanical stimuli to biochemical signals remain elusive because of a lack of appropriate *in vitro* models. At the molecular level, osteocytes are thought to regulate the response

* This work was supported, in whole or in part, by National Institutes of Health Grants AR059655 from the NIAMS (to P. D. P.) and DK011794 (to H. M. K.) and DK100215 (to M. N. W.) from the NIDDK. P. Babij was employed by Amgen Inc. and received Amgen stock.

¹ Supported by a Northrop Grumman Aerospace Systems Ph.D. training fellowship, a Massachusetts Institute of Technology Hugh Hampton Young fellowship, the National Space Biomedical Research Institute through NASA Grant NCC 9-58, and the United States Army Institute for Environmental Medicine Oak Ridge Science Institute for Science and Education fellowship program.

² Supported by Spain's Ministerio de Economía e Innovación (Grant SAF2013-43302-R), Posimat, and Fundacio Empreses Institut Químic de Sarrià.

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of bone to mechanical loading by at least two key molecules, sclerostin and receptor activator of nuclear factor κ B ligand (*RANKL*)⁴ (9, 13). Mature osteocytes are one of the few cells that postnatally produce sclerostin, which is encoded by the *SOST* gene. Sclerostin inhibits bone formation both *in vitro* and *in vivo* by directly reducing proliferation and differentiation of osteoblasts via the canonical Wnt signaling pathway. Sclerostin is thought to act by binding low density lipoprotein receptors 5 and 6 to inhibit Wnt- β -catenin signaling (14–16). Moreover, sclerostin appears central to the response of bone to mechanical loading. *SOST*/sclerostin expression increases with mechanical unloading (10, 17) and decreases with loading (10). In addition, *SOST* knock-out mice are resistant to disuse-induced bone loss (18), and mice treated with sclerostin antibody show an anabolic response in the hind limb unloaded model (19). Furthermore, serum sclerostin is significantly increased during prolonged (90-day) bed rest in healthy volunteers (17), in obese patients undergoing weight loss (20), and acutely in postmenopausal stroke patients (21). In addition to the effects of sclerostin, it was recently shown that soluble *RANKL* also secreted by osteocytes (9, 13) contributes to the control of bone remodeling. However, *RANKL* has also been found to be expressed in a variety of other cell types including osteoblasts, bone lining cells, keratinocytes, T and B lymphocytes, mammary epithelial cells, and undefined cell types within the brain (22). Thus, it is currently unknown whether osteocytes can increase *RANKL* in a cell-autonomous manner, thus potentially serving as an initiator of the cascade of bone resorption seen in mechanical unloading and microgravity.

Regardless of the initiation mechanisms, the hallmark of immobilization and microgravity in humans is an increase in bone resorption (23, 24), resulting in subsequent transient hypercalcemia with persistently increased urinary and fecal calcium loss (23). The endocrine counter-regulatory mechanisms to maintain normal serum calcium are a reduction in serum parathyroid hormone (PTH) and consequently lower 1,25-dihydroxyvitamin D concentrations (23). However, PTH is also a known potent regulator of *SOST*/sclerostin in osteocytes both in humans and in animal models (25, 26), raising the possibility that the increase in *SOST*/sclerostin during unloading or bed rest might be a consequence of decreased serum PTH rather than direct mechanical sensing by osteocytes. Indeed, there is an inverse correlation between PTH and sclerostin in male hypoparathyroid subjects (27), and PTH infusion in healthy men induces a decline in circulating sclerostin (28). Both *in vivo* and *in vitro*, PTH decreases sclerostin expression via activation of the PTH receptor expressed on osteocytes (29), and mice lacking the PTH receptor specifically in osteocytes have elevated expression of sclerostin (30). Thus, *in vivo* studies cannot determine whether suppression of PTH or other changes in cytokines, such as prostaglandin E₂ (PGE₂), are driving the increases in serum sclerostin following unloading. More broadly, there is no evidence to assess whether the increase in *SOST*/sclerostin is a direct osteocyte response to mechanical

unloading as postulated by the mechanostat theory proposed by Harold Frost (31).

Currently available osteocytic cell lines express basally very low levels of *SOST*/sclerostin and require high cell density with extended time in culture under differentiation conditions to produce detectable *SOST*/sclerostin (32–34), thus limiting their use for investigating mechanotransduction signaling pathways. To investigate osteocyte responses to unloading, we have isolated and characterized a novel osteocytic cell line (Ocy454), reported herein, that faithfully recapitulates the *in vivo* response of osteocytes to mechanical stimuli. Ocy454 cells show rapid, high level expression of *SOST*/sclerostin that is responsive to hormonal (PTH), cytokine (PGE₂), and mechanical stimuli. Furthermore, G_s α knockdown in Ocy454 led to significant increases in *SOST* expression matching known osteocyte *in vivo* regulation (35), demonstrating the broad utility of this new osteocytic cell line for studying *SOST*/sclerostin regulation as we have recently reported (36). Ocy454 also showed an enhanced osteocytic phenotype when cultured on a three-dimensional biomaterial by increasing *FGF23* expression upon PTH stimulation, highlighting the importance of optimizing *in vitro* culture conditions for studying certain aspects of osteocyte biology.

The primary hypothesis and objective of this study were to determine whether mechanical unloading is sensed in an osteocyte-endogenous manner and investigate the cellular mechanism(s) osteocytes utilize to regulate *SOST*/sclerostin. We hypothesized that simulated unloading (microgravity) as achieved in the NASA rotating wall bioreactors would increase *SOST*/sclerostin in a cell-autonomous fashion and that this increase would be suppressible by negative regulators (PTH and PGE₂) of *SOST*/sclerostin. As reported herein, osteocytic cells are indeed capable of responding to reduced mechanical forces with time-dependent increases in *SOST*/sclerostin expression. In addition, the gene expression profile in simulated microgravity (e.g. *SOST*, osteocalcin, *Phex*, and *MEPE*) is distinct from that seen with mechanical loading as achieved by fluid shear stress. Moreover, the increase in *SOST*/sclerostin expression is suppressed by PTH and PGE₂, suggesting upstream mechanistic overlap between mechanical sensing and G-protein-coupled receptor signaling and the potential to use targeted therapies in these signaling pathways as treatments for disuse-induced bone loss.

Experimental Procedures

Osteocytic Cell Lines—Mice expressing the green fluorescent protein (*GFP*) under the control of dentin matrix protein 1 (8-kb *DMPI-GFP*) (kindly provided by Dr. Ivo Kalajzic, University of Connecticut Health Center) (37) were mated with mice carrying a ubiquitously expressed SV40 large T antigen (Immortomouse, Charles River), and osteocytes were isolated from the long bones of 4-week-old double transgenic mice. Long bones were cut at the epiphysis; flushed with medium (α -minimum Eagle's medium) (Gibco) supplemented with 0.1% bovine serum albumin, 25 mM HEPES (pH 7.4) and containing 1 mg/ml collagenase type I:II (ratio, 1:3) (Worthington); and subjected to four sequential collagenase digestions, one EDTA digestion, and a final sixth collagenase digestion, and

⁴ The abbreviations used are: *RANKL*, receptor activator of nuclear factor κ B ligand; PTH, parathyroid hormone; OPG, *osteoprotegerin*; PGE₂, prostaglandin E₂; *DMPI*, dentin matrix protein 1; hPTH, human PTH.

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minced bone fragments were placed in collagen-coated 100-mm tissue discs. Cells were allowed to reach confluence at 33 °C and then grown for an additional 10–12 days at 37 °C prior to FACS for *DMPI-GFP* expression. Bulk-sorted *GFP*-positive cells were maintained on collagen-coated flasks grown in α -minimum Eagle's medium supplemented with 10% FBS (Gibco) and 1% antibiotic-antimycotic (Gibco). Subsequently, two criteria were selected for further identification of a mature osteocytic cell line: sorted *GFP*-positive were required to 1) have high levels of production of known osteocytic genes (*SOST* and *DMPI*) at the early time point of 14 days at the semipermissive temperature in the absence of differentiation and 2) respond to the known effects of PTH stimulation by suppression of *SOST* and increased expression of *RANKL*. This method provided a heterogeneous population of *DMPI-GFP*-positive cells that more faithfully resemble osteocytes *in vivo*, which are known to be a mixture of cells with various degrees of *SOST* and *DMPI* expression depending on their age/maturation. We performed our experiments in this heterogeneous population. In an effort to establish a more homogeneous osteocytic population, we also performed FACS on *Ocy454* to isolate single cell subclones. *Ocy454* and several single cell clones (36) have the same osteocyte marker expression and hormonal (PTH, PGE₂, and shear stress) response.

For two-dimensional cell culture, cells (*Ocy454*, IDG-SW3 (33), and primary long bone osteoblasts isolated from 4-week-old SV40 large T antigen mice) were plated at 10⁵ cells/ml and allowed to reach confluence at the permissive temperature (33 °C) for 3 days. Subsequently, cells were either differentiated at the permissive temperature or switched to the semipermissive temperature (37 °C) for the indicated time points. MLO-Y4 cells were plated at 10⁵ cells/ml, and RNA was extracted at 4 days (32). For primary osteocytes, cells were isolated from 4-week-old *DMPI-GFP* long bones. In brief, long bones were flushed of bone marrow with PBS, subjected to sequential collagenase digestions, and minced, and bone chips were placed in tissue culture plates. Subsequently, at the 2-week time point, cells were subjected to FACS. *GFP*[−] and *GFP*⁺ populations were directly collected into RNA extraction buffer (Qiagen).

The routine culturing conditions to maintain the *Ocy454* osteocytic phenotype were twice weekly subpassages (1:5) for up to 4 months from a frozen stock. For three-dimensional cell culture, 1.6 × 10⁶ *Ocy454* cells were plated on 200- μ m polystyrene Alvetex (Reinervate) well insert scaffolds. Scaffolds were collagen-coated according to the manufacturer's protocols for the indicated experiments. All other chemicals were from Sigma-Aldrich or Fisher Scientific.

Quantitative Real Time PCR—Total RNA was isolated (RNAEasy, Qiagen, Valencia, CA) according to the manufacturer's recommendations, and RNA was quantified (NanoDrop, Thermo Scientific, Rockford, IL). cDNA synthesis was performed (Qiagen or Taraka Clontech) on 0.5–1 μ g of total RNA followed by SYBR quantitative PCR (StepOnePlus, Life Technologies). Primer sequences are available upon request. β -Actin (*ACTB*) or *HPRT1* was used for normalization of gene expression. Δ CT was computed within each sample to the housekeeping reference, and $\Delta\Delta$ CT was computed across

experimental conditions. Experiments were run in triplicates unless otherwise indicated.

Western Blot—Whole cell lysates (Mammalian Protein Extraction Reagent, Thermo Scientific) from two-dimensional cell culture conditions were prepared according to the manufacturer's recommendations. Protein concentrations were quantified (Bio-Rad Protein Assay, Bio-Rad), and 10 μ g was separated on a 4–20% Tris-glycine denaturing gel (Life Technologies) and transferred to a PVDF membrane using the Trans-Blot Turbo (Bio-Rad) system according to the manufacturer's recommendations. The membrane was blocked with 3% BSA and 5% nonfat milk in Tris-buffered saline containing 0.05% Tween 20 (TBST) for 1 h and then incubated with goat polyclonal mouse sclerostin antibody (1:200; R&D Systems, Minneapolis, MN) overnight at 4 °C (30). After washing, secondary antibody (1:5000) was incubated for 1 h at room temperature and then developed using enhanced chemiluminescence (Thermo Scientific) (30). For G_s α immunoblotting, similar procedures were followed using an anti-G_s α antibody (Millipore, catalogue number 06-237).

Sclerostin Immunohistochemistry—Three-dimensional scaffolds were washed once with phosphate-buffered saline (Life Technologies) and frozen embedded (OCT, Tissue Tek), and 10- μ m sections were cut onto standard microscope slides. In brief, proteinase K was used for antigen retrieval for 15 min followed by a quench in 3% H₂O₂, methanol for 10 min, washing in H₂O, and rinsing in 1× TBS. Next, biotinylated anti-sclerostin antibody (R&D Systems, BAF1589) diluted 1:50 in Tris-NaCl blocking buffer was incubated for 1 h and washed three times with 1× Tris-NaCl-Tween buffer. Streptavidin-HRP diluted 1:100 in Tris-NaCl blocking buffer was then added to slides and incubated for 30 min, washed three times with 1× Tris-NaCl-Tween buffer, and incubated with 3,3'-diaminobenzidine HRP substrate (Vector Labs) for 5 min, and the slide was coverslipped.

Sclerostin ELISA—Four milliliters of cell culture supernatants from slow turning rotating wall bioreactor experiments at the indicated time points were spun at 850 rpm for 4 min, and the volume was reduced to 250 μ l with a 10-kDa centrifugal filter unit (Millipore, Billerica, MA) according to the manufacturer's recommendations. Supernatants were assayed for sclerostin using a commercially available assay (ALPCO, Salem, NH) according to the manufacturer's recommendations. For additional sclerostin ELISA experiments, an antibody matched pair ELISA was used (34). In brief, for the matched pair sclerostin ELISA, conditioned medium (36–48 h) was harvested from *Ocy454* cells as indicated in the figure legends and stored at −80 °C until further use. High binding 96-well plates (Fisher, 21-377-203) were coated with sclerostin antibody VI capture antibody (3 μ g/ml) in PBS for 1 h at room temperature. Plates were washed (PBS plus 0.5% Tween 20) and blocked with wash buffer supplemented with 1% BSA and 1% normal goat serum for 1 h at room temperature. Samples (60 μ l/well) were then added along with a standard curve of murine recombinant sclerostin (ALPCO), and plates were incubated overnight at 4 °C. Plates were washed three times and incubated with HRP-coupled sclerostin antibody VII detection antibody (0.5 μ g/ml) for 1 h at room temperature. After washing, signal detection

TABLE 1
shRNA target sequences

shRNA	Target sequences
<i>LacZ</i>	CCAACGTGACCTATCCCATTA
Luciferase	AGAATCGTCGTATGTCAGTGAA
GNAS E3	CGCAGATAAGAAACGCAGCAA
GNAS B2	GCCAAGTACTTCATTGCGGAT
GNAS G2	TCCGGATGAGTTTCTGAGAAAT
GNAS G9	CCTGCATGTTAATGGGTTTAA
GNAS C2	CCTGAAGAATCTGTGCCATT

was performed using Ultra 3,3',5,5'-tetramethylbenzidine ELISA (Pierce, 34028), stopped by 2 N sulfuric acid, and read at 450 nm. Prior to harvesting supernatant, cell number per well was always determined using the PrestoBlue assay (Life Technologies) according to the manufacturer's instructions.

For shRNA experiments, shRNA (Broad Institute, Cambridge, MA) lentiviral particles in puromycin-resistant vector targeted against luciferase (control; shLuciferase) or sh*G_sα* were used to infect cells plated 1 day prior at 0.5×10^5 cells/ml. Subsequently, infected cells were puromycin-selected (2 μg/ml) at the permissive temperature (33 °C) for 7 days and subsequently allowed to differentiate for 14–16 days at the semipermissive temperature. Table 1 provides the shRNA target sequences.

Simulated Microgravity—Ocy454 cells were plated on three-dimensional scaffolds as described above and allowed to grow at the permissive temperature (33 °C) for 3 days. Subsequently, scaffolds were moved to the semipermissive temperature (37 °C) for an additional culturing time before being loaded into the bioreactor. Scaffolds were cut into 3-mm discs using disposable biopsy punches (Integra Miltex, Plainsboro, NJ) and placed into non-rotating (static) or rotating (simulated microgravity) 110-ml slow turning lateral vessels (Synthecon, Houston, TX) for 3 days. For the rotating vessels, rotation speed was set to 18.6 rpm for the first 24 h and increased to 20.9 rpm to maintain solid body rotation kinetics throughout the experiment (38).

Two-dimensional Laminar Fluid Shear Stress—Ocy454 cells were plated on glass microscope culture slides (Flexcell International Corp.) at 2×10^5 cells/ml and allowed to grow at the permissive temperature (33 °C) for 3 days. Subsequently, slides were moved to the semipermissive temperature (37 °C) for an additional culturing time (11–14 days). Medium was changed for static slides, or slides were loaded into the laminar fluid flow shear stress device (Flexcell Streamer, Flexcell International Corp.) connected to an electronically controlled peristaltic pump with pulse dampers integrated into the flow circuit to allow for continuous unidirectional shear stress. Cells were exposed to 0.5 or 2 dynes/cm² for 2 h or 3 days (39–41).

Three-dimensional Fluid Shear Stress—Alvetex scaffolds were seeded with 1.6×10^6 cells and allowed to grow at the permissive temperature (33 °C) for 2 days prior to transferring to (37 °C) for differentiation. Cells were differentiated for 14 days prior to transferring to the Reinnervate perfusion plate. The perfusion plates were attached to a Masterflex peristaltic pump (catalog number 7520-57) with a Masterflex standard pump head (catalog number 7014-20) and exposed to either 0.5 or 2 dynes/cm² for either 1 or 3 days.

Statistical Analysis—All values are reported as the mean ± S.D. unless otherwise noted. Group mean differences were eval-

uated with Student's *t* test and considered significant at $p < 0.05$.

Results

Osteocytic (Ocy454) Cell Line Basal and Hormonal Characterization—Our method for osteocyte cell line development coupled fluorescent sorting for an osteocytic marker (*DMP1*) with functional hormonal screening to accurately ensure the cell line possessed the key functional responses of mature osteocytes *in vivo*. Of several preparations, one population of sorted *DMP-GFP-SV40* large T antigen (Ocy454) cells was selected for further characterization on the basis of its high expression of *SOST* at early time points at the semipermissive temperature. Ocy454 osteocytic cells displayed a dendritic morphology (Fig. 1A) similar to other osteocytic cell lines (32, 33) and at 2 weeks at the semipermissive temperature (37 °C) expressed the *DMP1-GFP* transgene (Fig. 1, B and C).

After 2 weeks at 37 °C, Ocy454 cells expressed significantly higher levels of *SOST* and *DMP1* compared with long bone primary osteocytes as well as the only other available osteocytic cell lines, MLO-Y4 and IDG-SW3 (Fig. 2, A and B). Upon further study, we also observed that Ocy454 differentiated upon contact inhibition at the permissive temperature (Figs. 1C and 2B). However, Ocy454 differentiated at a slower pace at the permissive temperature. For example, at the 1-week time point, there were lower levels of *SOST* at the permissive temperature compared with the semipermissive temperature (Fig. 2B). In addition, Ocy454 expressed levels of *SOST* that were significantly higher than those expressed by long bone osteoblasts (Fig. 2B) as early as 1 week at 37 °C in the absence of differentiation factors. Sclerostin was detected by ELISA in the cell culture supernatant at day 11, and its concentration continued to increase with time in culture (Fig. 2B). Furthermore, after 2 weeks at the semipermissive temperature (37 °C), Ocy454 cells expressed high levels of other characteristic osteocytic genes, such as *DMP1* (Fig. 2B). In contrast, these cells had low levels of expression of genes characteristic of immature osteocytes and late osteoblasts, such as keratocan (Fig. 2B) (42, 43). After 1 week in culture at 37 °C, Ocy454 cells expressed levels of *DMP1* (Fig. 2B) that were significantly higher than those expressed by long bone osteoblasts. In addition, *RANKL* was highly expressed at the permissive temperature, and then expression dropped to levels comparable with wild-type osteoblasts and the IDG-SW3 cell line with differentiation at the semipermissive temperature (Fig. 2B). Interestingly, the expression of *FGF23* in Ocy454 followed a biphasic pattern of expression with significantly more mRNA at 1 week in semipermissive culture than at later time points (Fig. 2B).

We next assessed Ocy454 cell responsiveness to known osteocyte regulators. Short term (4-h) treatment with human (h)PTH(1–34), forskolin, or (16-h) PGE₂ induced a statistically significant down-regulation of *SOST* (Fig. 3A; $p < 0.001$ for all) and sclerostin both in whole cell lysate and conditioned medium (Fig. 3, B and C). These results are consistent with the known inhibitory effects of these agents on *SOST* expression. In contrast, a PGE₂ inhibitor, indomethacin, caused an increase in *SOST* (Fig. 3B), showing that Ocy454 cells have an intact hormonal axis that increases *SOST* expression.

Osteocyte-autonomous Responses to Mechanical Unloading

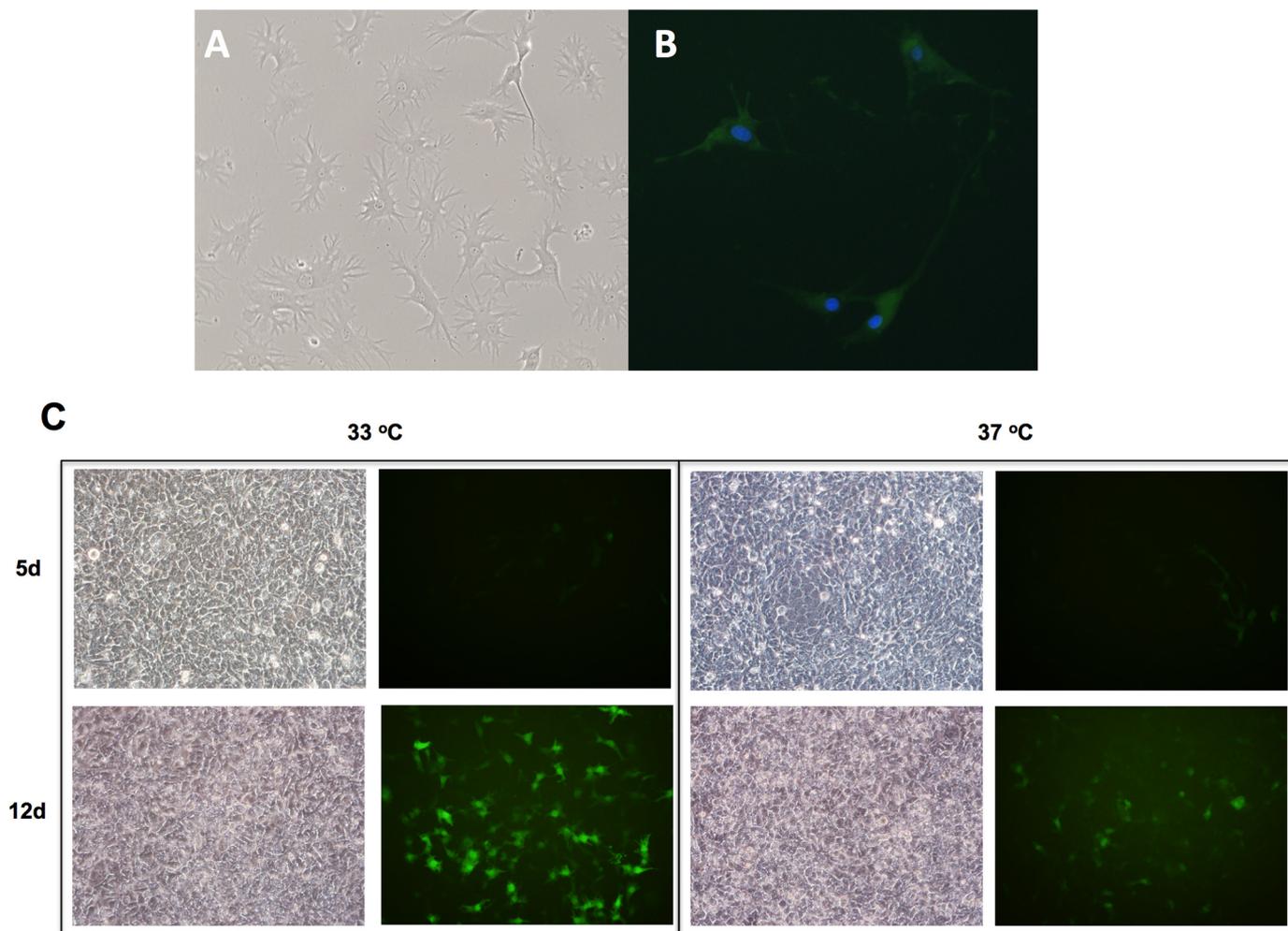


FIGURE 1. *A*, representative dendritic morphology of osteocytic cell line Ocy454. *B*, *DMP1-GFP* expression at 3 days for permissive temperature (33 °C). *C*, *DMP1-GFP* expression time course at 5 and 12 days (*d*) for both permissive (33 °C) and semipermissive temperature (37 °C).

In addition, hPTH(1–34) dose- and time-response experiments showed Ocy454 to be sensitive to down-regulation of *SOST* in as short as 2 h (100 nM; Fig. 3*D*) and a 50% suppression at doses as low as 0.1 nM hPTH(1–34) (Fig. 3*D*). Similarly, hPTH(1–34) (4 h), forskolin, and PGE₂ caused concurrent increases in *RANKL* mRNA (Fig. 3*E*). hPTH(1–34) suppressed *Mef2C* mRNA (Fig. 3*F*), consistent with previous reports (44, 45), and *DMP1* mRNA (Fig. 3*G*). There was no regulation of *FGF23* mRNA by 4-h PTH treatment in Ocy454 at 1 or 2 weeks in two-dimensional non-collagen- and collagen-coated 6-well plate culture conditions (data not shown).

We and others have previously reported that mice lacking (35, 46) *G_sα* have increased levels of *SOST*/sclerostin. To confirm these *in vivo* results in Ocy454 cells, we used shRNA to knock down *G_sα* in Ocy454 as was done previously for *HDAC5* (36). The range of sclerostin secretion (normalized to cell number) was determined in each experiment using 10 separate control lentiviruses expressing shRNAs against non-expressed genes (*LacZ*, luciferase, *GFP*, and red fluorescent protein). *Dotted lines* indicate two standard deviations above the mean value of sclerostin secretion (normalized to cell number) in the presence of the control hairpins. As shown in Fig. 4*A*, two of five

hairpins tested to achieve lentivirus-mediated shRNA knock-down of *GNAS* (but not related heterotrimeric G-proteins *GNAQ* and *GNA11*) consistently increased sclerostin secretion (individual hairpins labeled next to corresponding data points). The individual hairpins that reduced *GNAS* mRNA levels accordingly increased *SOST* expression (Fig. 4*B*), thereby confirming the expected knockdown/phenotype relationship for this known *SOST* regulator. *GNAS* hairpins “G2” and “G9” both effectively reduced *G_sα* protein levels (Fig. 4*C*), and hairpin G2 was selected for further study. Sclerostin secretion in control (shLuciferase) and *GNAS* G2 shRNA-expressing cells was determined over time. As shown in Fig. 4*D*, *GNAS* shRNA causes an increase in sclerostin secretion at all time points with the most dramatic results at early times after switching cells from 33 to 37 °C. Finally, *GNAS* shRNA cells were tested for PTH responsiveness. Fig. 4*E* shows that *GNAS* shRNA increases basal *SOST* expression (after 14 days at 37 °C); furthermore, whereas control cells respond to PTH at this time point with suppression of *SOST* levels, this is not the case when *G_sα* levels are reduced. Taken together, these data confirm a cell-intrinsic role for *G_sα* in osteocytes and further support the use of Ocy454 cells for studying *SOST* gene regulation.

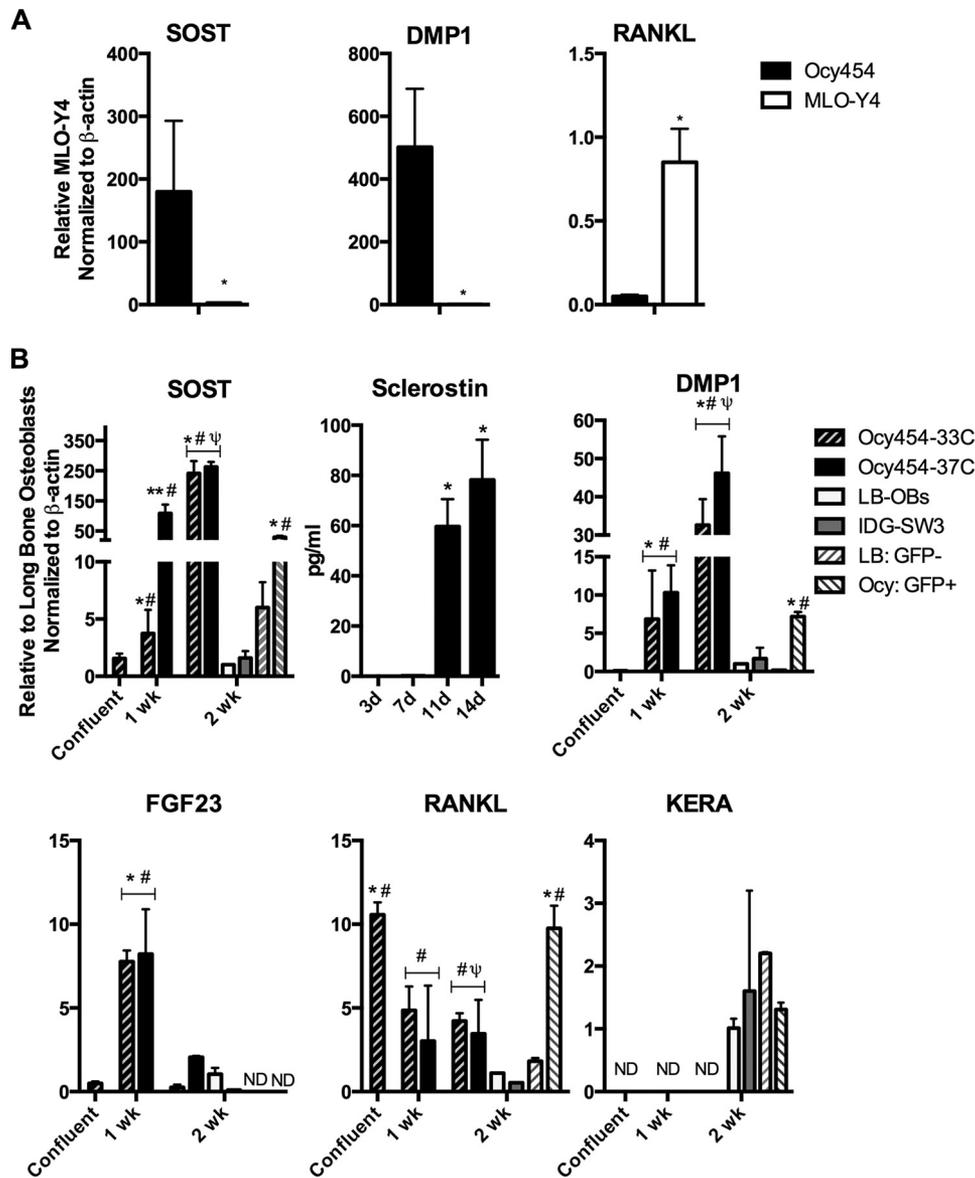


FIGURE 2. *A*, Ocy454 at 2 weeks (37 °C) (black bars) express characteristic osteocytic markers versus MLO-Y4 in the absence of differentiation medium. *B*, Ocy454 (Ocy) at 1 and 2 weeks (wk) (37 °C) (black bars) express characteristic osteocytic markers *SOST*, sclerostin, *DMP1*, *FGF23*, and *RANKL* and lack keratocan (*KERA*) expression in the absence of differentiation medium compared with long bone osteoblasts (LB-OBs), IDG-SW3 (2 weeks), long bone (LB) *DMP1*-GFP⁻ and long bone *DMP1*-GFP⁺ osteocytes. *, $p < 0.001$ for 1 and 2 weeks at semipermissive growth temperature (37 °C) versus permissive growth temperature (33 °C; 3 days (d)); **, $p < 0.001$ for 1 and 2 weeks at semipermissive temperature versus permissive growth temperature at the indicated time points; #, $p < 0.001$ for Ocy454 versus long bone osteoblasts; Ψ , $p < 0.001$ for Ocy454 versus long bone *DMP1*-GFP⁺ osteocytes at the indicated time points. ND, not detected. Error bars represent S.D. of 1.

Three-dimensional Culture Enhances Osteocytic Phenotype—To evaluate the effects of a three-dimensional culture environment on the expression of osteocyte-specific genes and to provide a scaffold for cell attachment in the rotating wall bioreactor system used to simulate microgravity, Ocy454 cells were seeded onto scaffolds and cultured for an additional 7–14 days. Consistent with our two-dimensional culture results, we also observed a significant down-regulation of *SOST* (Fig. 5A), increases in *RANKL* (Fig. 5B), and decreases in *DMP1* (Fig. 5D) in three-dimensional cultures ($p < 0.001$ for all) upon PTH treatment. Previous reports have demonstrated that TGF β ₁ increases *SOST*/sclerostin levels during mechanical loading (47, 48). In contrast to prior reports, treatment of Ocy454 cells with TGF β ₁ (10 ng/ml; 24 h) resulted in a down-regulation of

SOST (Fig. 5A) and increases in *RANKL* (Fig. 5B), and a known TGF β ₁-responsive gene, *Serpine1*, increased 2.3 ± 0.1 -fold ($p < 0.007$). Interestingly, in contrast to two-dimensional cultures, culture in three dimensions with 4-h PTH treatment resulted in a 5-fold ($p < 0.001$) increase in *FGF23* expression (Fig. 5C). In a direct comparison between three-dimensional and two-dimensional culture at an early time point (3 days at 37 °C), Ocy454 had significantly higher amounts of *SOST* and *RANKL* in the three-dimensional culture conditions (Fig. 5G) than in the two-dimensional setting. Furthermore, Ocy454 displayed dendritic morphology in three-dimensional culture conditions (Fig. 5E), and we observed decreases in sclerostin protein expression with hPTH(1–34) treatment in three-dimensional culture (Fig. 5F).

Osteocyte-autonomous Responses to Mechanical Unloading

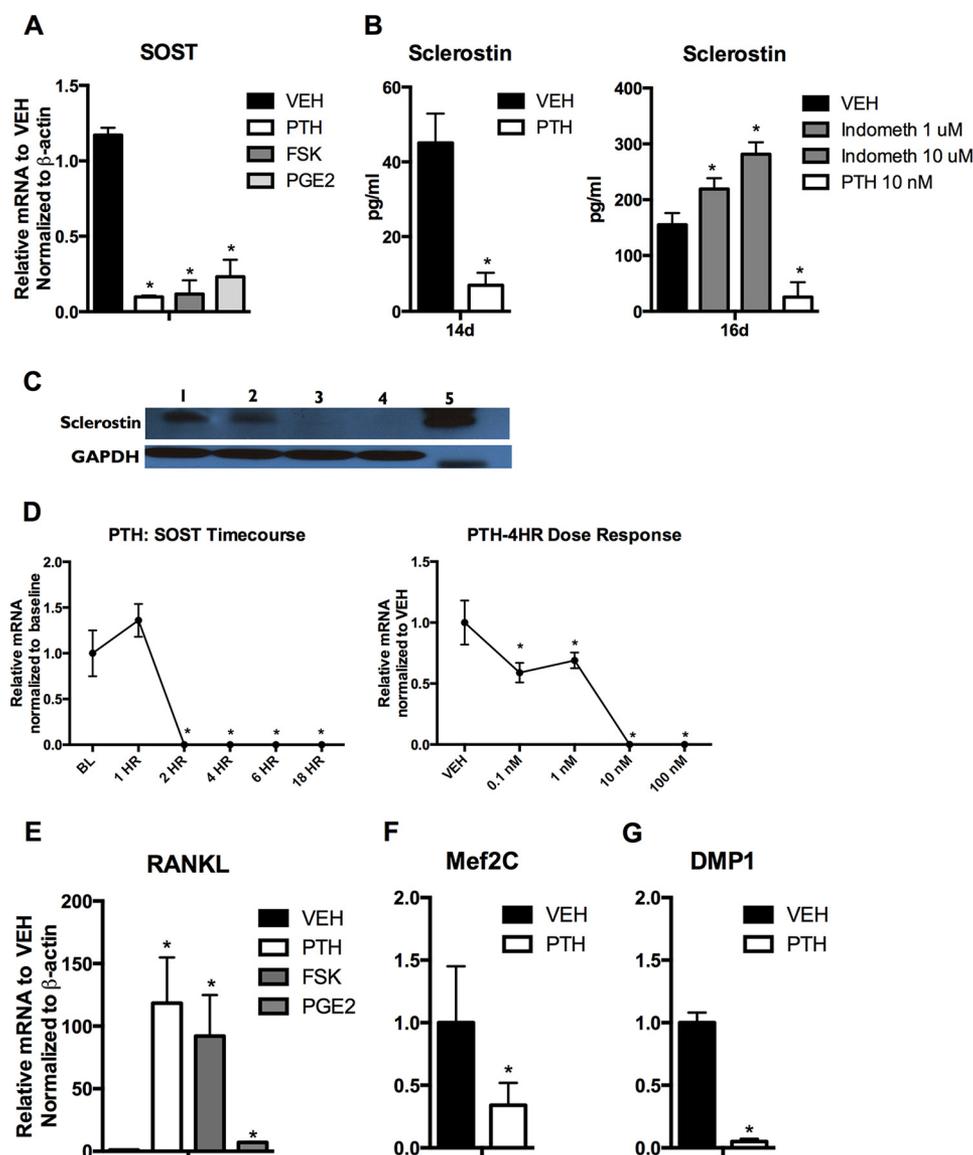


FIGURE 3. *A*, Ocy454 cells show decreased *SOST* expression after treatment with PTH(1–34) (4 h, 100 nM), forskolin (4 h, 10 μ M), PGE₂ (16 h, 100 nM) at 2 weeks at semipermissive temperature. *B*, 16-h hPTH(1–34) (100 nM) treatment decreases secreted sclerostin as measured by ELISA (ALPCO), and 48-h indomethacin (*Indometh*) treatment (1 and 10 μ M) increases secreted sclerostin by ELISA (Amgen). *C*, 4-h hPTH(1–34) (100 nM) treatment of Ocy454 at 2 weeks suppresses total cell lysate sclerostin. *Lanes 1 and 2*, vehicle (VEH); *lanes 3 and 4*, hPTH(1–34); *lane 5*, sclerostin standard (APLCO). *D*, hPTH(1–34) time course and dose response for *SOST* suppression. *E*, 4-h treatment to hPTH(1–34), forskolin, and 16-h PGE₂ increases *RANKL* at 2 weeks. Four-hour hPTH(1–34) treatment suppresses *Mef2C* (*F*) and *DMP1* (*G*). *, $p < 0.001$ for all *SOST* time courses and hormone/cytokine treatments versus vehicle. Error bars represent S.D. of 1. *d*, days.

Fluid Shear Stress Regulation of Ocy454 in Two-dimensional Culture—Ocy454 were then subjected to continuous unidirectional fluid shear stress in two-dimensional culture conditions. Consistent with previous reports using UMR 106.01 osteoblast-like cells (39), short term (2-h) fluid shear stress significantly suppressed *SOST* mRNA levels at low and high shear stresses (Fig. 6A). Whereas *RANKL* was reduced at low shear stress (0.5–2 dynes/cm²), *RANKL* and *DMP1* were increased at higher shear stress (8 dynes/cm²) as shown in Fig. 6, B and C. These results demonstrate that Ocy454 cells are exquisitely responsive to mechanical forces with intact *SOST*, *DMP1*, and *RANKL* regulation to overloading stimuli. Our results also suggest differential regulation of *SOST* and *DMP1* to fluid shear stress but not to simulated microgravity, whereas the response to hPTH(1–34) is the same.

Simulated Microgravity Increases *SOST*/*Sclerostin* and *RANKL*—We then utilized the NASA-developed rotating wall bioreactor system to mimic microgravity to assess whether osteocytes can directly sense mechanical unloading and regulate the expression of sclerostin and *RANKL*, which are known to be involved in the response of bone to unloading. Indeed, under simulated microgravity conditions (3 days), there was a statistically significant increase of 3.5 ± 1.9 -fold ($p < 0.001$) in *SOST* expression compared with static controls (Fig. 7A). Secreted sclerostin as assessed by ELISA was also increased by 1.4 ± 0.1 as early as 1 day, 2.7 ± 0.4 at 2 days, and 4.7 ± 0.1 at 3 days ($p < 0.001$ for all) (Fig. 7B). There were no significant changes in other osteoblastic genes (osteocalcin, alkaline phosphatase, and osterix mRNAs) between the loaded and unloaded bioreactors, demonstrating that the increase in

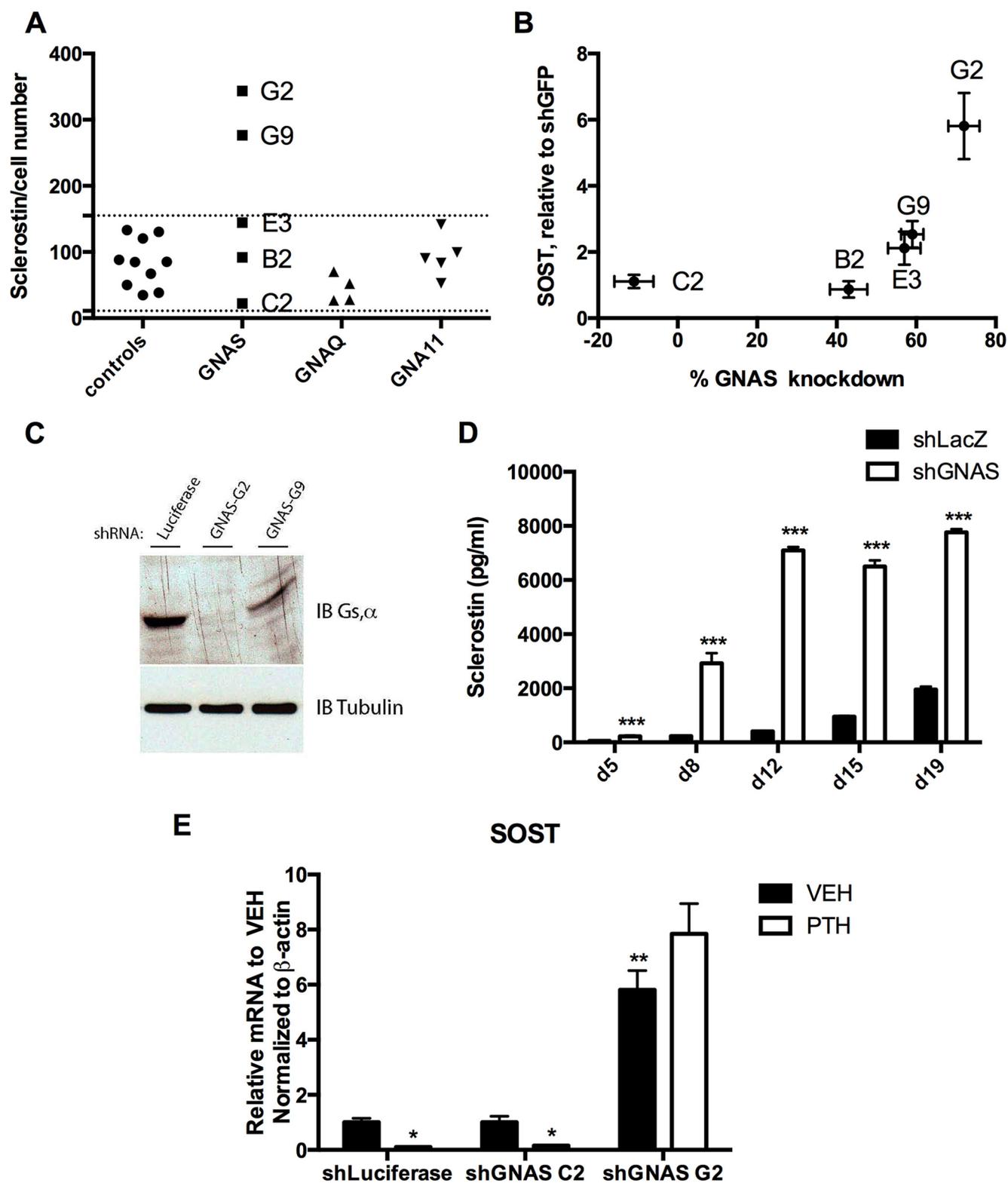


FIGURE 4. *A*, Ocy454 cells were infected with control shRNA-expressing lentiviruses (shGFP, shLuciferase, shRed fluorescent protein, and shLacZ) and five separate hairpins targeting the indicated gene. Each data point represents sclerostin/cell number values obtained for an individual hairpin. Dotted lines indicate values two standard deviations above and below those of the controls. For *GNAS*, individual hairpins are labeled on the data plot. *B*, Ocy454 cells were infected with shGFP and the indicated *GNAS* shRNA lentiviruses and then switched to 37 °C. 14 days later, RNA was isolated, and RT-quantitative PCR was performed for β -actin, *GNAS*, and *SOST*. *C*, as in *B* except lysates were generated for immunoblotting. *D*, as in *B* except conditioned medium was collected at the indicated times for sclerostin ELISA. *E*, as in *B* expect cells were treated with vehicle or hPTH(1–34) (50 nM) for 4 h followed by semi-quantitative PCR for *SOST* and β -actin. *, $p < 0.01$ for hPTH(1–34) versus vehicle (VEH); **, $p < 0.001$ for shGNAS G2 versus shLuciferase and shGNAS C2; ***, $p < 0.001$ for shGNAS versus shLacZ for all time points. Error bars represent one S.D.

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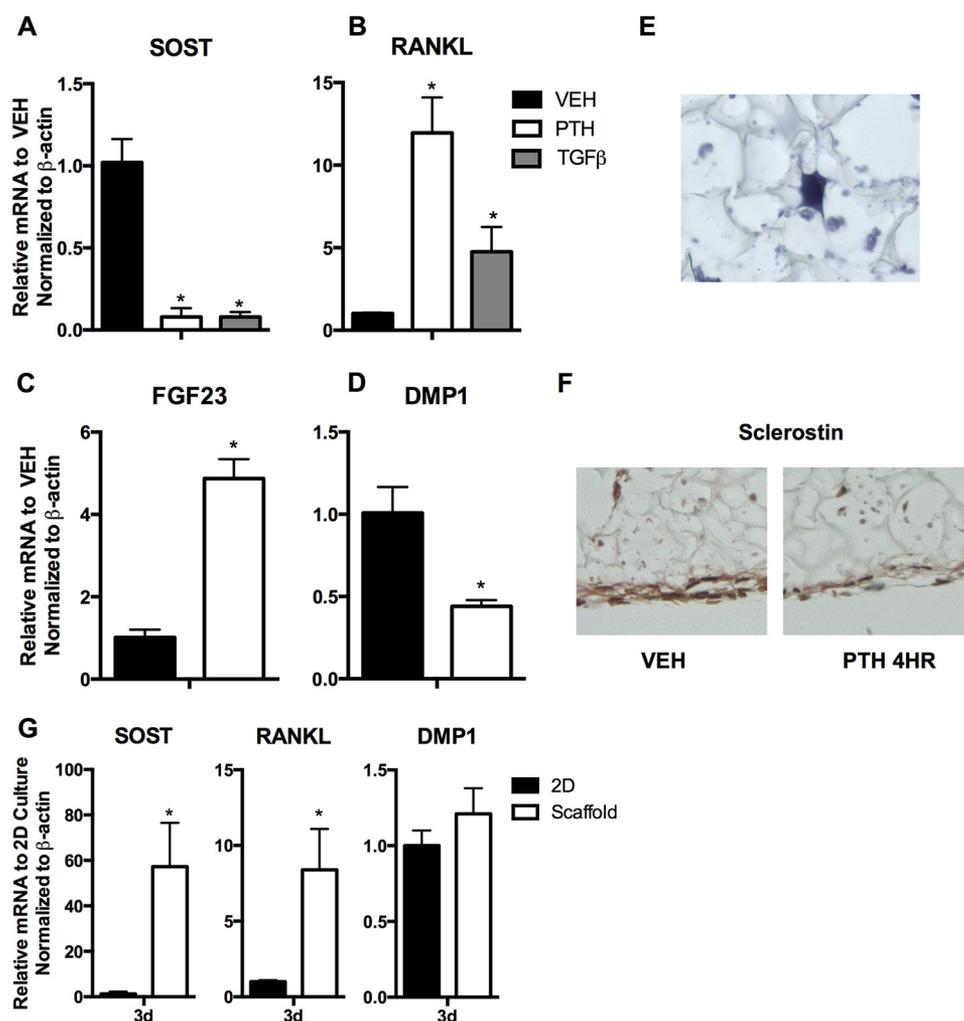


FIGURE 5. Ocy454 cells were grown on collagen-coated (A–D) three-dimensional scaffold (for hPTH(1–34) experiments). Four-hour hPTH(1–34) (100 nm) and 24-h TGF β ₁ (10 ng/ml) treatment at 12–14 days decreases *SOST* (A) and increases *RANKL* (B). Four-hour hPTH(1–34) increases *FGF23* (C) and decreases *DMP1* (D) expression. E, representative H&E stain of Ocy454 cell within the scaffold. F, 4-h hPTH(1–34) (100 nm) treatment decreases sclerostin expression of Ocy454 cells on the scaffold. G, Ocy454 gene expression for *SOST*, *DMP1*, and *RANKL* on three-dimensional scaffolds versus two-dimensional (2D) culture at semipermissive growth temperature for 3 days (d) (37 °C). *, $p < 0.001$ for hPTH(1–34) or $p < 0.007$ for TGF β ₁ versus vehicle (VEH). Error bars represent S.D. of 1.

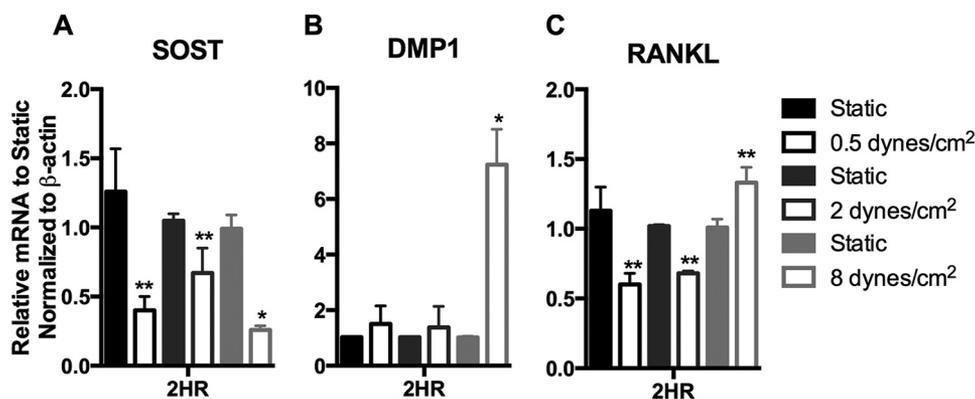


FIGURE 6. Short term (2-h) fluid shear stress in two-dimensional culture reduces *SOST* (A), increases *DMP1* at high shear stress (8 dynes/cm²) (B), and reduces *RANKL* at low shear stress (0.5–2 dynes/cm²) and increases *RANKL* at high shear stress (8 dyne/cm²) (C). *, $p < 0.001$; **, $p < 0.05$ for static versus fluid shear stress. Error bars represent S.D. of 1.

SOST/sclerostin expression was not a consequence of an altered cell state as we observed in our prolonged two-dimensional fluid shear stress experiments. In an effort to identify upstream regulator of *SOST*/sclerostin expression, we assessed changes in reported and potential regulators of

SOST in the *Mef2* pathway (*Mef2A–D*), PGE₂ pathway (*mPTGES-1*, *15-HGPD*, *EP2*, and *EP4*), *SIRT1*, osterix, *PTHrP*, PTH receptor, and periostin. We observed no changes in mRNA levels for any of these known regulators of *SOST* (Table 2) following simulated microgravity.

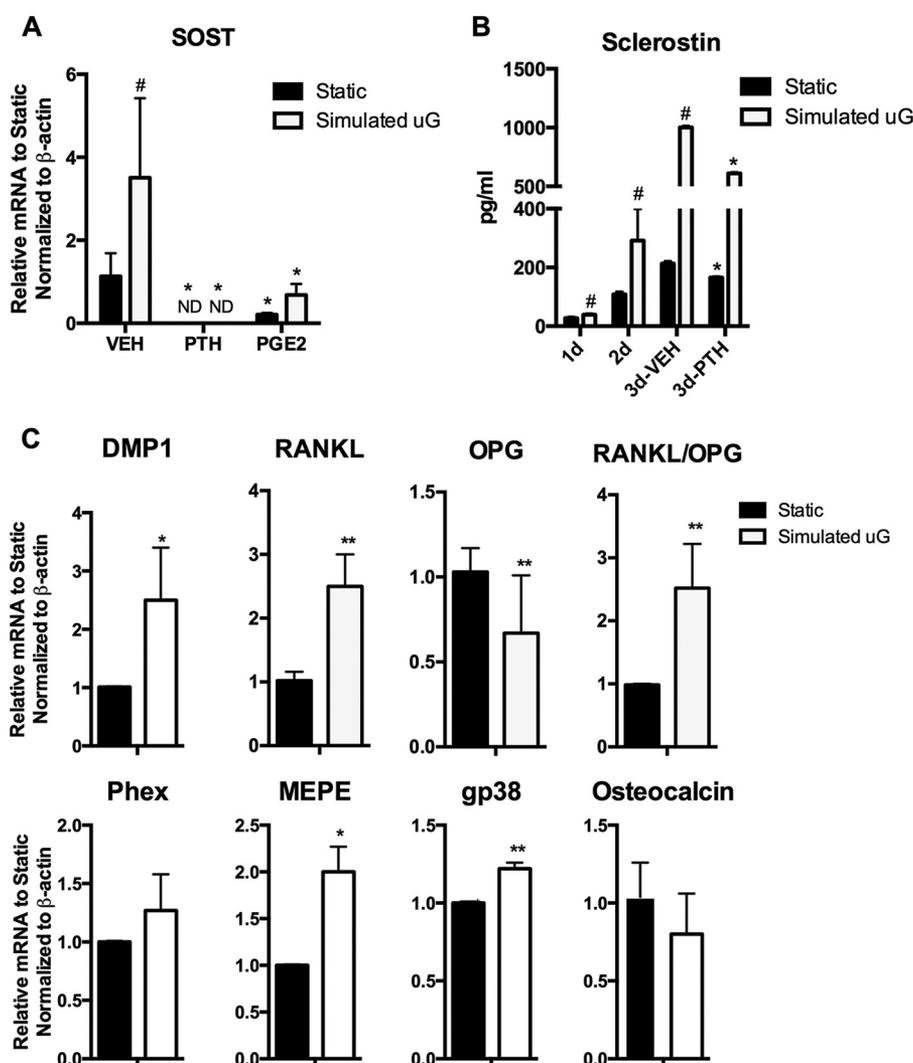


FIGURE 7. *A*, 3-day simulated microgravity (white bars) increases *SOST* compared with static controls (black bars), and 4-h hPTH(1–34) (50 nM) and 16-h PGE₂ (5 nM) decrease *SOST* in both simulated microgravity (uG) and static controls. *B*, sclerostin increases as early as 1 day (d) of exposure to simulated microgravity and remains elevated through 3 days. Overnight (16-h) hPTH(1–34) (50 nM) treatment on days 2–3 suppresses secreted sclerostin as measured by ELISA (APLCO). *C*, 3-day simulated microgravity increases *DMP1*, *RANKL*, *RANKL/OPG* ratio, *gp38*, and *MEPE*; decreases *OPG*; and has no effect on *Phex* or osteocalcin. #, $p < 0.001$; **, $p < 0.05$ for simulated microgravity versus static controls; *, $p < 0.001$ for all hormone/cytokine treatments versus vehicle (VEH). ND, not detected. Error bars represent S.D. of 1.

Consistent with previous reports of osteoblasts increasing *RANKL* expression in simulated microgravity conditions (49), we observed increased *RANKL* mRNA (Fig. 7C) and a concurrent modest reduction in *OPG* mRNA (Fig. 7C), resulting in a statistically significant increase in the *RANKL/OPG* ratio in unloaded versus static conditions (Fig. 7C). We also detected a modest increase on mRNAs encoding *DMPI*, *MEPE*, and *gp38* with no change in *Phex* or osteocalcin mRNA under simulated microgravity conditions (Fig. 7C). Thus, we report these regulatory changes to osteocytic genes as a signature of osteocytes exposed to simulated microgravity.

G-protein-coupled Receptor Responsiveness: *SOST/Sclerostin* in Simulated Microgravity—To determine whether activation of PTH receptors (or other G-protein-coupled receptors) could still suppress *SOST/sclerostin* in microgravity, we tested the effects of PTH and PGE₂ treatment in simulated microgravity. PTH (Fig. 7A) suppressed *SOST* and sclerostin levels of expression (Fig. 7B) to the same extent in static and unloaded condi-

tions ($p < 0.001$). Similarly, PGE₂ caused the same magnitude of suppression of *SOST* expression in both static and simulated microgravity conditions. These results demonstrate that, although the increase in *SOST* expression is not dependent on reductions in G-protein-coupled receptor expression (PTH receptor and EP2/4) or *G_s* activity (Table 2), modulating G-protein-coupled receptor signaling can still regulate *SOST/sclerostin* expression in the setting of microgravity or unloading, such as disuse.

Long Term Fluid Shear Stress Regulation of *Ocy454*—One limitation of the NASA rotating wall bioreactor system is the possible generation of minimal fluid shear stress demonstrated to be on the order of 0.5–2 dynes/cm² (38, 50). To investigate whether the changes in gene expression observed in the NASA bioreactor were indeed due to simulated microgravity and not minimal shear stress, we subjected *Ocy454* cells to long term exposure (1 or 3 days) to low laminar fluid shear stresses (0.5–2 dynes/cm²) in three-dimensional (Alvetex) culture condi-

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TABLE 2
Evaluated regulators of *SOST*/sclerostin in simulated microgravity

ECR5 enhancers <i>Mef2A</i> , - <i>C</i> , - <i>D</i> ; <i>Mef2B</i> (not expressed) (34, 45, 67)
<i>SOST</i> promoter transcription factors <i>TFGB1</i> (47, 48) Osterix (59) <i>Runx2</i> (68) <i>SIRT1</i> (58) <i>Pax6</i> (51) Periostin (44) <i>MyoD</i> : not expressed (68) <i>G_sα</i> (35, 46)
PGE₂ pathway <i>EP2</i> , <i>EP4</i> (54, 56) <i>Cox-2</i> <i>mPTGES-1</i> <i>15-HGPD</i>
Cell membrane receptors <i>PTH1R</i> <i>PTHrP</i> : not expressed <i>P2XR1-7</i>

tions. At 2 dynes/cm², we observed a significant reduction in *SOST* mRNA and no change in *DMPI* mRNA at 1 day (Fig. 8). At 0.5 dyne/cm², we observed significant suppression of *SOST* mRNA; a significant increase in *DMPI* mRNA; and decreases in *OPG*, *MEPE*, *gp38* (1 day), and osteocalcin mRNAs with no effect on *RANKL* or *Phex* mRNA (Fig. 8). Similar results for 2 dynes/cm² were observed at 3 days (Fig. 8) with the exception of a lack of regulation of *DMPI* mRNA. These data clearly indicated that the up-regulation of *SOST*/sclerostin present in the NASA rotating wall bioreactor system was indeed due to simulated microgravity and not minimal shear stress.

In addition, as shown in Fig. 9, we subjected Ocy454 to two-dimensional long term low fluid flow. These low flow conditions induced changes in the differentiation state of Ocy454 as illustrated by significantly elevated levels of expression of *SOST*, *DMPI*, *RANKL*, *OPG* (3 days), *Phex*, *MEPE*, and *gp38* with a reduction of osteocalcin expression (Fig. 9). Overall, these two-dimensional and three-dimensional long term mechanical overloading results demonstrated that our simulated microgravity experiments reflect a unique osteocyte cellular response to mechanical unloading stimuli.

Discussion

The primary objective of this study was to determine whether increases in *SOST*/sclerostin and *RANKL* seen in the context of disuse-induced bone loss are an intrinsic osteocytic response to mechanical unloading. Although it has been established that osteocytes are key players in the response of bone to mechanical stimuli (10, 39, 40, 52, 53), it is still unclear whether their response to unloading is a direct response to reduction in load as theorized by Wolff's law or a consequence of changes in systemic endocrine or paracrine factors. Furthermore, the biochemical response of the osteocytic network to overloading (10, 39, 40) does not in itself provide evidence for a direct response to unloading stimuli. Here we present new data showing that osteocytes elicit an intrinsic response to mechanical loading that is independent of the known external hormonal influence of PTH and other factors.

Prior studies in rodents have reported increases in *SOST*/sclerostin in bone tissue (10) and in circulating sclerostin (19)

during unloading. In addition, increased circulating serum sclerostin levels with a concurrent reduction of PTH levels have been reported in the context of disuse-induced bone loss in rodents (55) and humans (17). However, as PTH is a strong negative regulator of *SOST*/sclerostin, these *in vivo* studies cannot address the question of whether osteocytes can directly sense mechanical unloading or respond to hormonal changes.

Importantly, our results suggest that the increase in bone resorption in mechanical unloading and microgravity with associated transient hypercalcemia and reduced parathyroid hormone levels is not the driving force for increases in *SOST*/sclerostin and *RANKL* expression. Thus, for the first time, we have observed isolated osteocytes sensing mechanical unloading and responding with increases in *SOST*/sclerostin and the *RANKL*/*OPG* ratio.

The transcriptional regulators of *SOST*/sclerostin in mechanical unloading are currently unknown. However, *Mef2* transcription factors have been shown in several contexts to bind a distal enhancer (ECR5) in the *SOST* locus, resulting in the increased expression of *SOST*/sclerostin (34, 45). However, we observed no transcriptional changes in the potential regulators of *SOST* in the *Mef2* pathway (*Mef2A*, -*C*, and -*D*) (Table 2). Furthermore, because PGE₂ is a known negative regulator of *SOST*/sclerostin in a *Mef2*-independent mechanism (56) and reductions in PGE₂ production genes (*Cox-2*) have been observed in osteoblasts exposed to microgravity (57), we assessed changes in the PGE₂ production and degradation pathways (*mPTGES-1* and *15-HGPD*) and receptor expression (*EP2* and *EP4*) as shown in Table 2. Notably, no changes in mRNA of transcripts responsible for PGE₂ production, PGE₂ degradation, or PGE₂ receptors were observed between static and unloaded cultures, implying that the increases of *SOST*/sclerostin in mechanical unloading are presumably not arising from changes in the PGE₂ pathway. Several transcription factors have also been reported to suppress the *SOST* promoter (like *SIRT1* and osterix) (58, 59) or act at the distal enhancer (ECR5) (like *TGFβ₁₋₃*) (47). However, in the context of mechanical unloading, we observed no change in *SIRT1*, osterix, or *TGFβ₁₋₃* mRNAs (Table 2). It has also been proposed that the periostin extracellular matrix protein suppresses *SOST* in a *Mef2C*-dependent mechanism that is regulated by PTH (44, 60). However, in Ocy454, we observed no correlation among sclerostin, PTH, and periostin mRNA or protein expression in two-dimensional cultures or in the context of mechanical unloading (data not shown). Thus, future studies investigating the novel transcriptional or post-transcriptional regulation of *SOST*/sclerostin in the context of mechanical unloading and microgravity are warranted.

G-protein-coupled hormonal (PTH) and cytokine regulators (PGE₂) were capable of suppressing the increases of *SOST*/sclerostin seen in mechanical unloading. Thus, although our results show that osteocytes can directly sense mechanical unloading, they also suggest that the overall level of sclerostin *in vivo* appears to be an integral response of the osteocyte network to mechanical loading, hormonal, and cytokine cues. Of particular note, we have shown that mice lacking PTH receptor in osteocytes lose bone in the hind limb unloading model, consistent with our *in vitro* findings that G-protein-coupled receptor

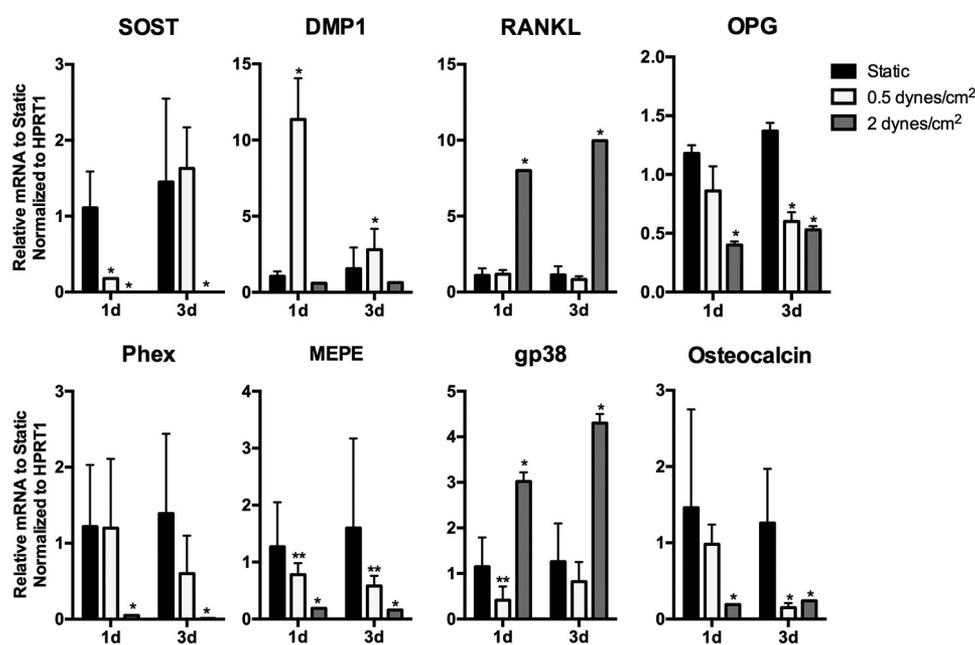


FIGURE 8. Fluid shear stress of Ocy454 in three-dimensional culture at 1 and 3 days (d). Fluid low shear stress of 0.5 and 2 dynes/cm² reduces *SOST* (A); increases *DMP1* (B); decreases *OPG* (C), *Phex* (D), and *MEPE* (E); increases *gp38* (F), and decreases osteocalcin (G) at the shear stresses and time points indicated. *, $p < 0.001$; **, $p < 0.05$ for static versus fluid shear stress. Error bars represent S.D. of 1.

signaling may play a minimal role in disuse-induced bone loss. One study has recently reported that *SOST* regulation in mechanical unloading in rodents could be site-specific with modest (-1.5%) down-regulation in cancellous metaphyseal and cortical bone, whereas up-regulation was seen in diaphyseal cortical (61) regions. Our results are consistent with these findings as our cell lines were isolated from the diaphysis of long bones. However, as the majority of osteocytes in the load-bearing skeleton are located in the diaphysis of long bones and circulating levels of sclerostin are elevated in the setting of disuse-induced bone loss, the clinical significance of the heterogeneous nature of the osteocytic network remains to be further explored. Furthermore, although the NASA rotating wall bioreactor provides a solid body rotation with a minimal fluid shear stress in the range of 0.5–2 dynes/cm² (38, 50), no currently existing *in vitro* ground-based model of microgravity can fully eliminate the low level of shear stress inherent in our model.

However, short mechanical loading (10, 62) and fluid shear stress (39) are known to cause decreased, not increased, levels of *SOST*/sclerostin and *RANKL* as we have observed (Fig. 7). To further investigate this confounding variable of minimal fluid shear stress in the NASA bioreactor, we subjected Ocy454 cells in two-dimensional and three-dimensional culture conditions to low unidirectional fluid shear stress. Importantly, neither two-dimensional nor three-dimensional fluid shear stress matched the pattern of osteocytic gene expression seen in simulated microgravity. In addition, cells on the surfaces of the scaffolds are likely exposed to shear stresses higher in range than cells within the scaffold. However, the same seeding technique was used in all scaffold experiments so non-uniformity in cell distribution could in and of itself not account for the significant down-regulation of *SOST* in three-dimensional fluid flow (Fig. 8) compared with the increase in *SOST* (Fig. 7) we

observed in the simulated microgravity experiments. Finally, additional variables, such as nutrient availability, could also be acting as confounding factors to our observed results. However, the simulated microgravity experiments utilized a 110-ml bioreactor. Daily changes of 10% volume of medium were also performed to facilitate elimination of bubbles. Thus, for the cell density and number, these culture conditions for both static and microgravity conditions are nutrient-rich. Our interpretation notwithstanding, we acknowledge that such confounding variables specific to osteocytic cell cultures in simulated microgravity will need to be addressed in future experiments under conditions of true microgravity.

To enable these studies, we generated a novel osteocytic cell line Ocy454 that recapitulates known *in vivo* osteocytic functions without the requirement for long term high density cultures and in the absence of differentiation medium. These cells were isolated from long bones of double transgenic mice expressing both a *GFP* under the *DMP1* promoter and a temperature-sensitive large T antigen. These cells can be cultured for a long period of time at permissive conditions (33 °C) without losing their phenotypic characteristics and then can rapidly recapitulate a mature osteocytic phenotype after 10–12 days in culture at semipermissive conditions (37 °C). As expected for an osteocyte, these cells express high levels of *SOST*/sclerostin, *DMP1*, *Phex*, and *E11*, whereas they have undetectable levels of the osteoblastic marker keratocan at all time points. Thus, in contrast to currently available osteocytic cell lines (MLO-Y4 and IDG-SW3 for example), the uniqueness of these cells is their expression of mature osteocytic genes in the absence of differentiation factors at early time points, suggesting that these cells display a mature osteocytic phenotype in a shorter experimental time frame. In addition, Ocy454 responded to short term mechanical overloading, achieved via both traditional two-dimensional laminar shear stress and three-di-

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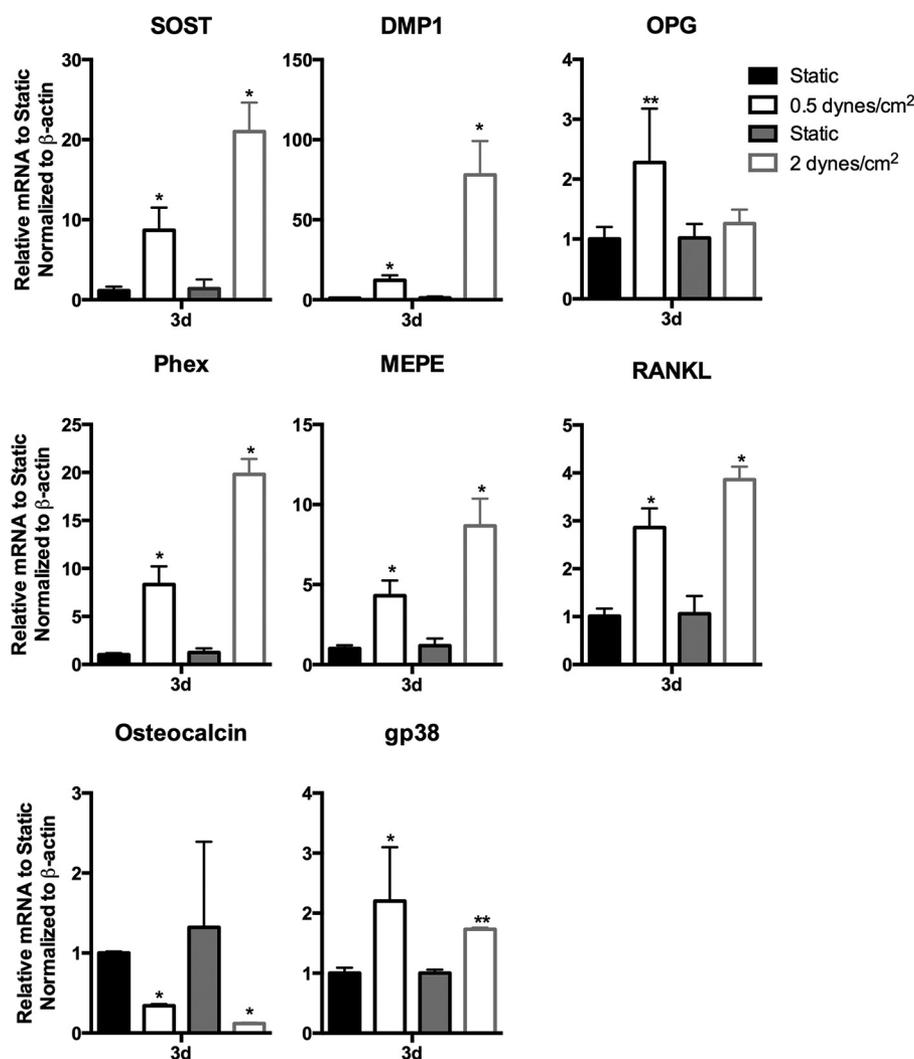


FIGURE 9. Long term (3-day) fluid shear stress in two-dimensional culture increases *SOST*, *DMP1*, *RANKL*, *OPG*, *Phex*, *MEPE*, and *gp38* and decreases osteocalcin at the indicated shear stresses and time points. *, $p < 0.001$; **, $p < 0.05$ for static versus fluid shear stress. Error bars represent S.D. of 1.

dimensional fluid shear stress, by reducing *SOST* as reported previously (39).

Interestingly, *RANKL* expression is higher at permissive conditions (more undifferentiated state), and this expression rapidly declines upon differentiation (2–3 days at 37 °C), suggesting that high *RANKL*-expressing cells might belong to a less mature “osteocytic” phenotype. Similar findings were evident for *FGF23* as well. In addition, consistent with prior reports that osteocytes have improved characteristics in three-dimensional culture conditions (63, 64), our osteocytic cell line exhibited increased *FGF23* upon PTH treatment in three-dimensional culture conditions but not two-dimensional culture conditions. It is well appreciated that for a wide variety of cell types three-dimensional cell cultures mimic to a greater degree the *in vivo* conditions by preserving the three-dimensional integrity of individual cells, allowing for cell aggregation and direct signaling and enabling cells to create their own niche microenvironment in conjunction with their extracellular matrix (65). Thus, our studies add to the growing body of evidence for the use of three-dimensional *in vitro* culture conditions to study certain aspects of osteocyte biology. For the experiments we have con-

ducted, our cell line faithfully reflects key characteristics of *bona fide in vivo* osteocytes.

In addition, we have also isolated another long bone cell line (Ocy491) (66) using this same technique, but it has the characteristics of a less mature osteocyte, requiring up to 21 days to produce appreciable levels of *SOST*, that could be useful for osteoblast-to-osteocyte differentiation studies. Thus, here we report the establishment of osteocyte cell lines that can be routinely cultured over short time periods with high level expression of *SOST*/sclerostin that is responsive to hormonal (PTH), cytokine, and mechanical stimuli, enabling a wide diversity of future studies on the regulation of mature osteocytes in other disease processes.

In conclusion, isolated osteocytes can directly sense a mechanical unloading stimulus, resulting in the increases in expression of both inhibitors of bone formation (*SOST*/sclerostin) and stimulators of bone resorption (notably *RANKL* and the *RANKL*/*OPG* ratio). Future therapies, aimed at modulating the gravity-sensing pathways of the osteocyte could lead to improved therapies for a range of bone disorders.

Acknowledgments—We acknowledge Dr. Stefan Przyborski for technical support of this work. We thank Drs. John Doench and David Root of the Broad Institute of Harvard and Massachusetts Institute of Technology (Cambridge, MA) for providing shRNA reagents and protocols; Dr. Lynda Bonewald for providing the MLO-Y4 and IDG-SW3 cell lines; and Drs. Julie Hughes, Stephen Muza, and Ronald Wayne Matheny for facilitating use of the Flexcell Streamer for this project.

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J. Biol. Chem. 2015, 290:16744-16758.

doi: 10.1074/jbc.M114.628313 originally published online May 7, 2015

Access the most updated version of this article at doi: [10.1074/jbc.M114.628313](https://doi.org/10.1074/jbc.M114.628313)

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